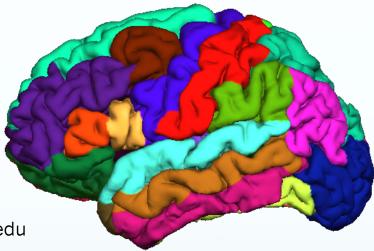


Longitudinal FreeSurfer



Martin Reuter mreuter@nmr.mgh.harvard.edu http://reuter.mit.edu

MGH/HST Athinoula A. Martinos Center for Biomedical Imaging

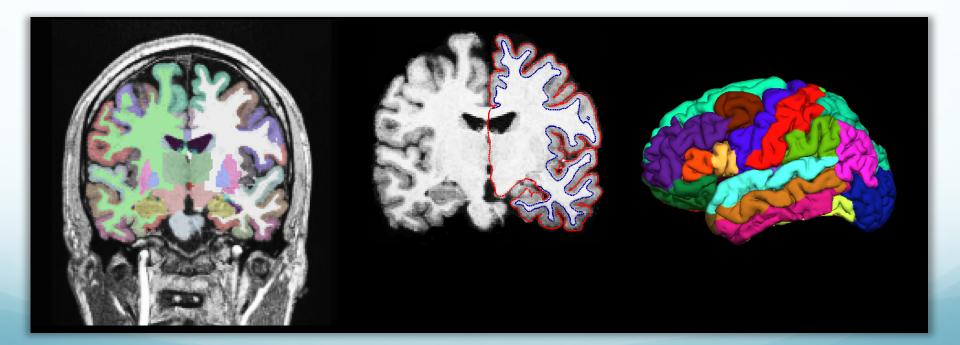




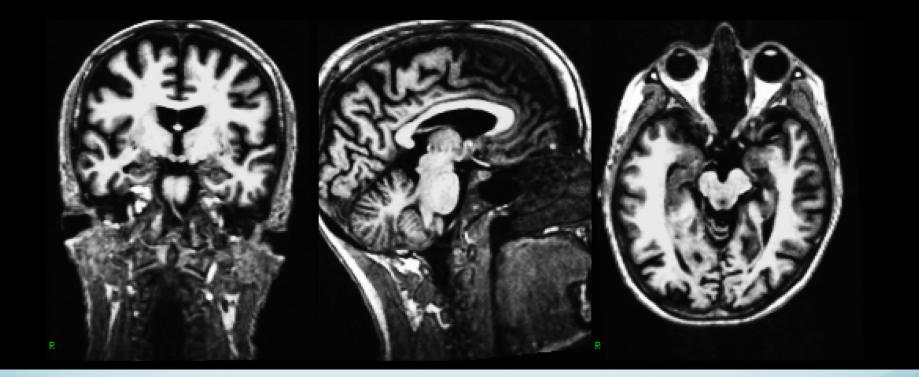


What can we do with FreeSurfer?

- measure volume of cortical or subcortical structures
- compute thickness (locally) of the cortical sheet
- study differences of populations (diseased, control)



Neurodegenerative disease:



14 time points, 6 years, Huntington's Disease

We'd like to:

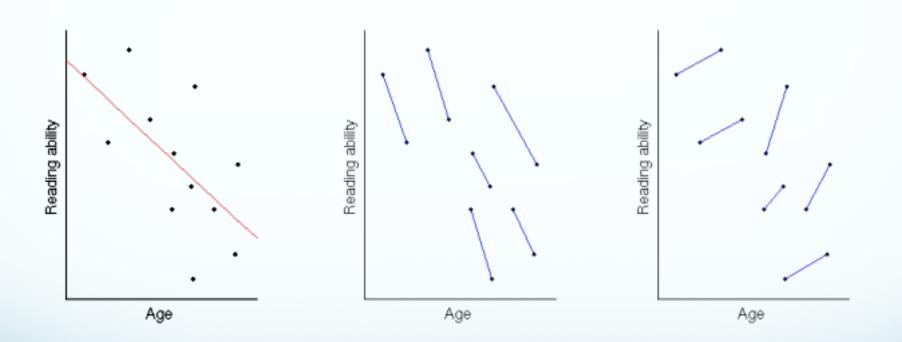
• exploit longitudinal information (same subject, different time points)

Why longitudinal?

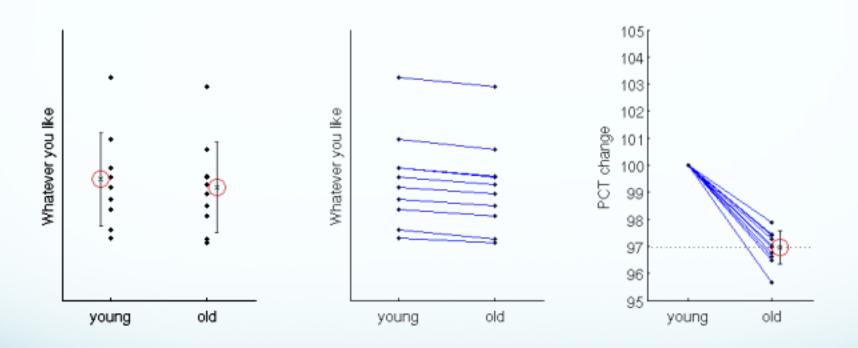
- to reduce variability on intra-individual morph. estimates
- to detect small changes, or use less subjects (power)
- for marker of disease progression (atrophy)
- to better estimate time to onset of symptoms
- to study effects of drug treatment

[Reuter et al, NeuroImage 2012]

Example 1



Example 2



Challenges in Longitudinal Designs

1. Over-Regularization:

- Temporal smoothing
- Non-linear warps
- Potentially underestimating change
- 2. Bias [Reuter and Fischl 2011], [Reuter et al. 2012]
 - Interpolation Asymmetries [Yushkevich et al. 2010]
 - Asymmetric Information Transfer
 - Often overestimating change
- 3. Limited designs:
 - Only 2 time points
 - Special purposes (e.g. only surfaces, WM/GM)

Reuter et al. NeuroImage 2011 & 2012

How can it be done?

• Stay *unbiased* with respect to any specific time point by <u>treating all the same</u>

- Create a within subject *template* (base) as an <u>initial</u> <u>guess</u> for segmentation and reconstruction
- Initialize each time point with the template to <u>reduce</u> <u>variability</u> in the optimization process
- For this we need a <u>robust registration</u> (rigid) and <u>template estimation</u>

Reuter et al. Neurolmage 2011 & 2012

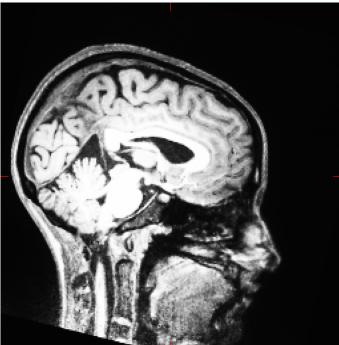
Goal: Highly accurate inverse consistent registrations

- In the **presence** of:
 - Noise
 - Gradient non-linearities
 - Movement: jaw, tongue, neck, eye, scalp ...
 - Cropping
 - Atrophy (or other longitudinal change)

We need:

- Inverse consistency keep registration unbiased
- Robust statistics to reduce influence of outliers



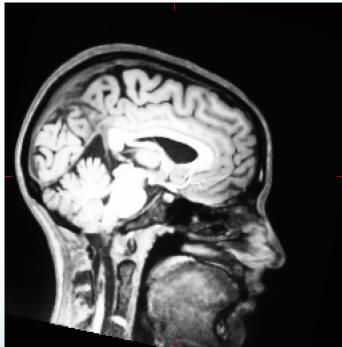


Target

Target

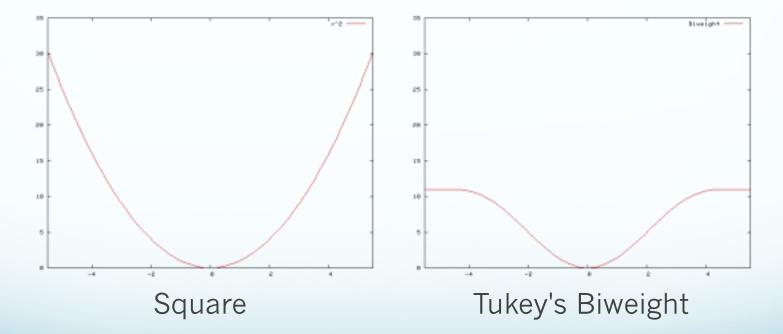


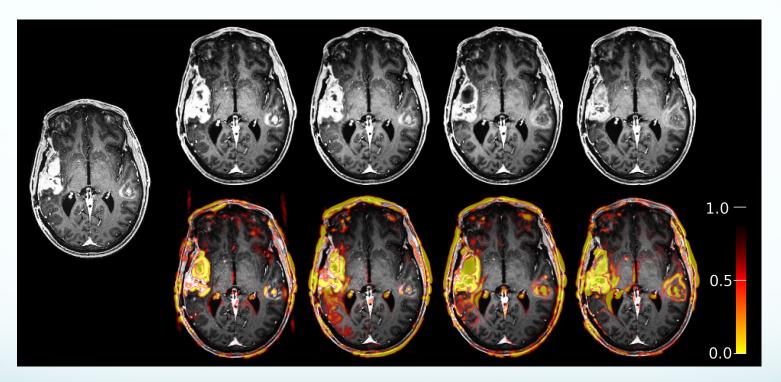
Registered Src FSL FLIRT



Registered Src Robust

Limited contribution of outliers [Nestares&Heeger 2000]





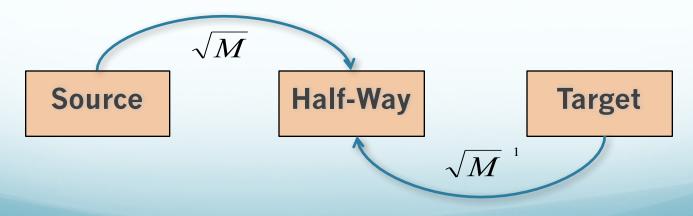
Tumor data with significant intensity differences in the brain, registered to first time point (left).

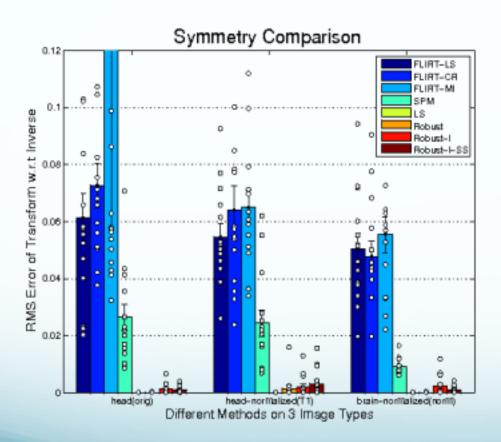
Inverse consistency:

• a symmetric displacement model:

$$r(p) = I^T \vec{x} + \frac{1}{2}\vec{d}(\vec{p}) = I^S \vec{x} + \frac{1}{2}\vec{d}(\vec{p})$$

 resample both source and target to an unbiased halfway space in intermediate steps (matrix square root)





Inverse consistency of different methods on original (orig), intensity normalized (T1) and skull stripped (norm) images.

LS and Robust:

• nearly perfect symmetry (worst case RMS < 0.02)

Other methods:

• several alignments with RMS errors > 0.1

- mri_robust_register is part of FreeSurfer
- can be used for pair-wise registration (optimally within subject, within modality)
- can output results in half-way space
- can output 'outlier-weights'
- see also Reuter et al. "Highly Accurate Inverse Consistent Registration: A Robust Approach", NeuroImage 2010. <u>http://reuter.mit.edu/publications/</u> for comparison with FLIRT (FSL) and SPM coreg.
- for more than 2 images use: mri_robust_template

Robust Template Estimation

- Minimization problem for N images: $\{\hat{I}, \hat{\varphi}_i\} := \underset{I, \varphi_i}{\operatorname{argmin}} \sum_{i=1}^{N} E(I_i \circ \varphi_i, I) + D(\varphi_i)^2$
- Image Dissimilarity:

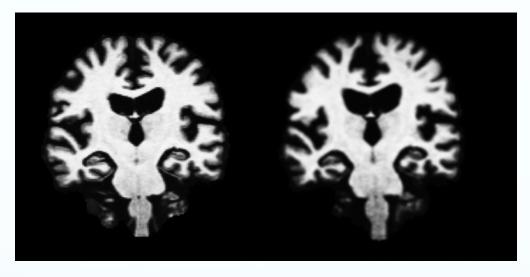
$$E(I_1, I_2) = \int_{\Omega} |I_1(x) - I_2(x)| \, dx$$

• Metric of Transformations: $D(\vec{t},r)^2 = \parallel \vec{t} \parallel^2 + \parallel R - \mathbf{1} \parallel_F^2$

Longitudinal Processing Challenges

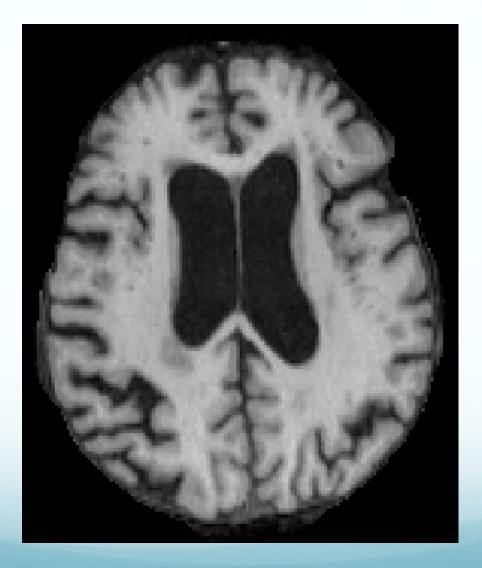
- **1.** Over-Regularization (limited flexibility):
 - > Will avoid by only initializing processing
- 2. Bias [Reuter and Fischl 2011], [Reuter et al. 2012]
 - Interpolation Asymmetries [Yushkevich et al. 2010]
 - Asymmetric Information Transfer
 - > Will avoid by treating time points the same
- 3. Limited designs:
 - Allow n time points
 - Reliably estimate all of FS measurements

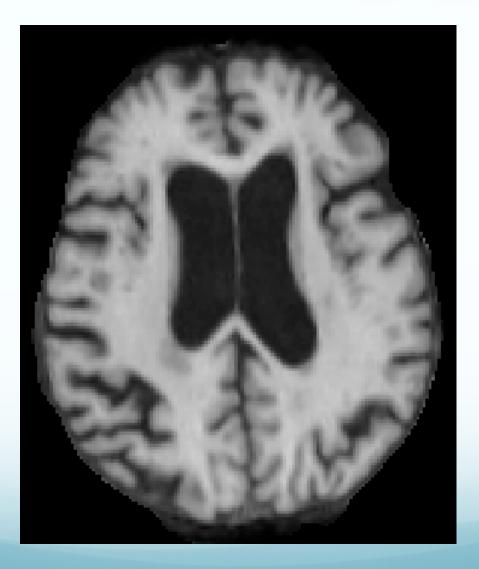
(i) Interpolation Asymmetries (Bias)

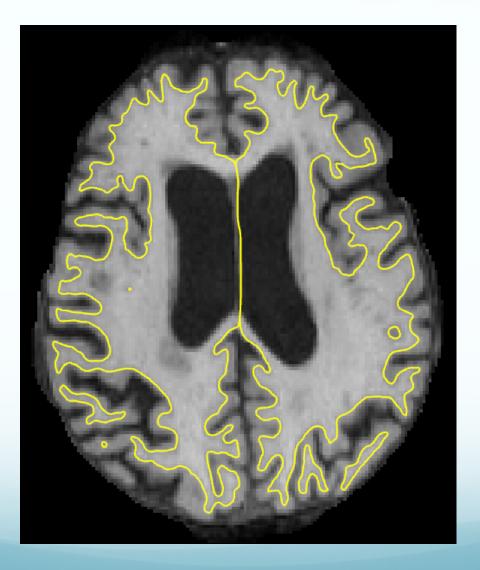


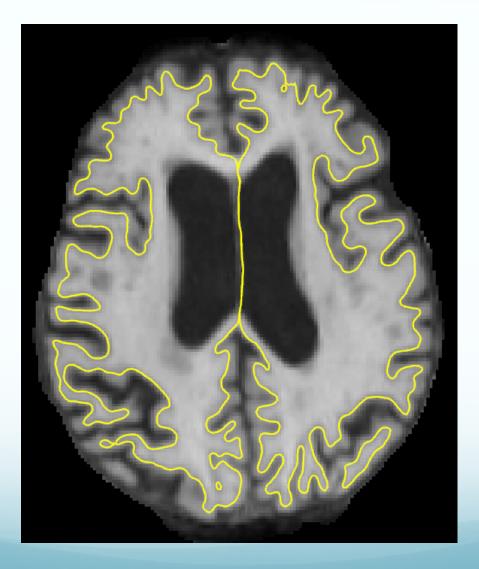
Mapping follow-up to baseline:

- Keeps baseline image fixed (crisp)
- Causes interpolation artefacts in follow-up (smoothing)
- Often leads to overestimating change

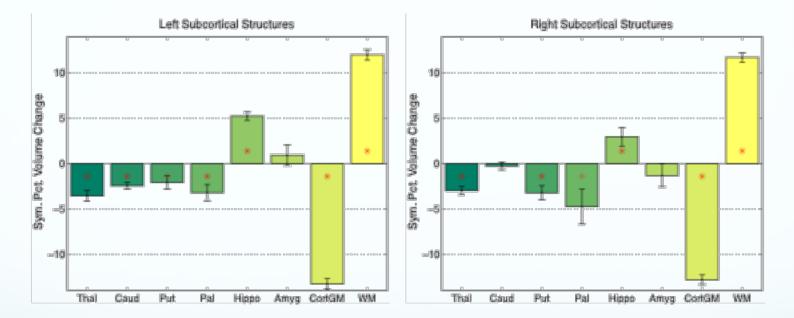








(i) Interpolation Asymmetries (Bias)

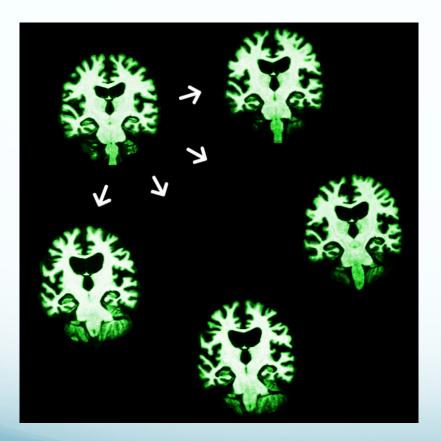


MIRIAD dataset: 65 subjects

First session first scan compared to twice interpolated image. Regional: not finding it does not mean it is not there.

http://miriad.drc.ion.ucl.ac.uk

(ii) Asymmetric Information Transfer



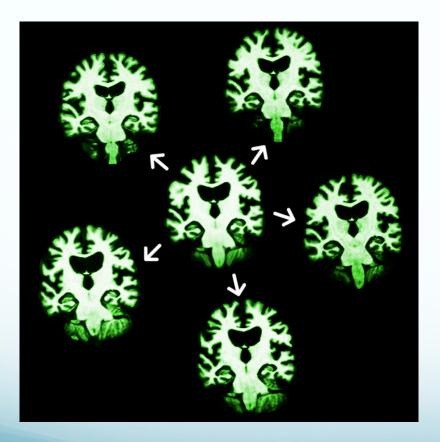
Example:

- 1. Process baseline
- 2. Transfer results from baseline to follow-up
- 3. Let procedures evolve in follow-up

(or construct skullstrip in baseline, or Talairach transform ...)

Can introduce bias!

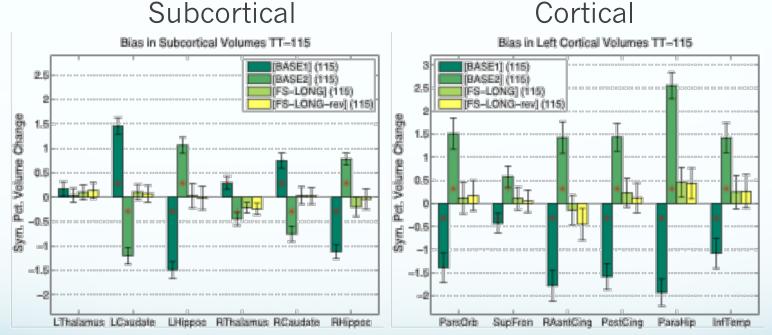
Robust Unbiased Subject Template



- Create subject template (iterative registration to median)
- 2. Process template
- 3. Transfer to time points
- 4. Let it evolve there
- All time points are treated the same
- Minimize overregularization by letting tps evolve freely

(ii) Asymmetric Information Transfer

Test-Retest (115 subjects, 2 scans, same session)



Biased information transfer: [BASE1] and [BASE2]. Our method [FS-LONG] [FS-LONG-rev] shows no bias.

Review the central ideas

Idea: Would like to include some information that much of the anatomy is the same over time, but don't want to lose sensitivity to disease effects.

How to minimize over regularization:

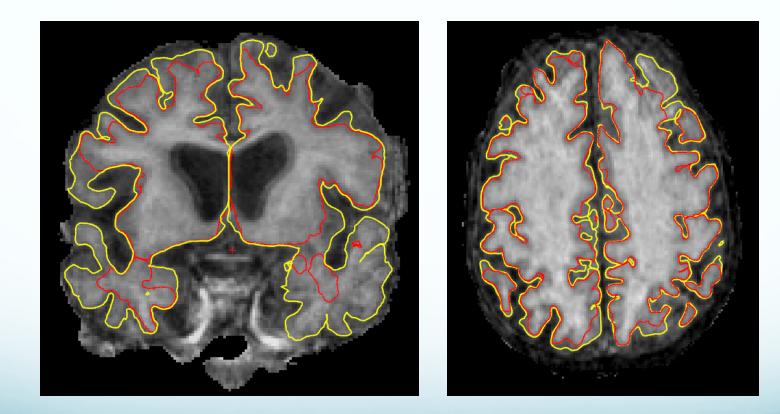
✓ Only initialize processing, evolve freely
 How to avoid processing bias:

✓ Treat all time points the same

Why not simply do independent processing then?

Sharing information across time points increases reliability, statistical power!

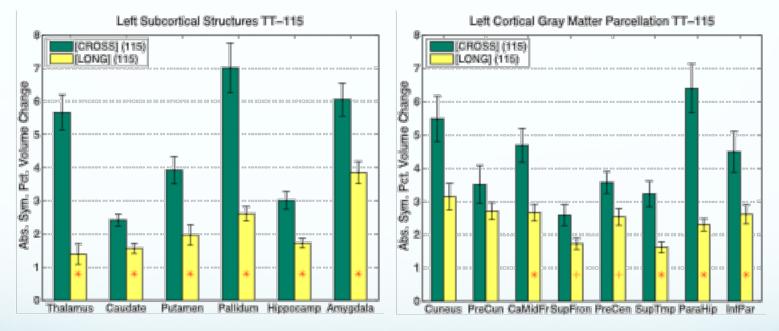
Improved Surface Placement



Test-Retest Reliability

Subcortical

Cortical

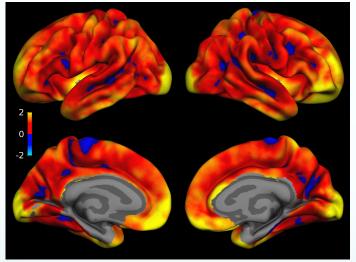


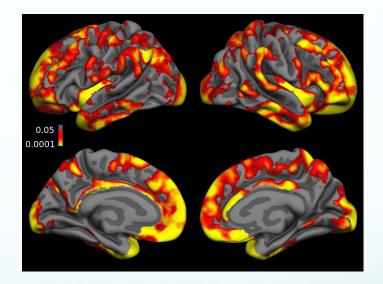
[LONG] significantly improves reliability 115 subjects, MEMPRAGE, 2 scans, same session

Test-Retest Reliability

Diff. ([CROSS]-[LONG]) of Abs. Thick. Change:

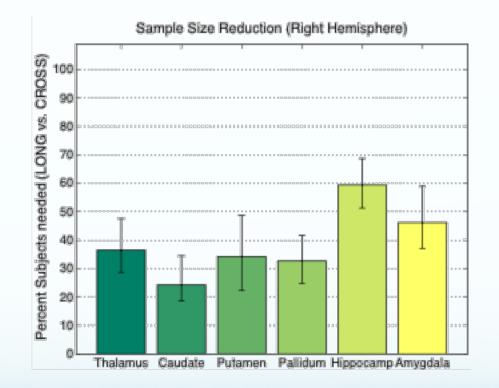
Significance Map





[LONG] significantly improves reliability 115 subjects, ME MPRAGE, 2 scans, same session

Increased Power

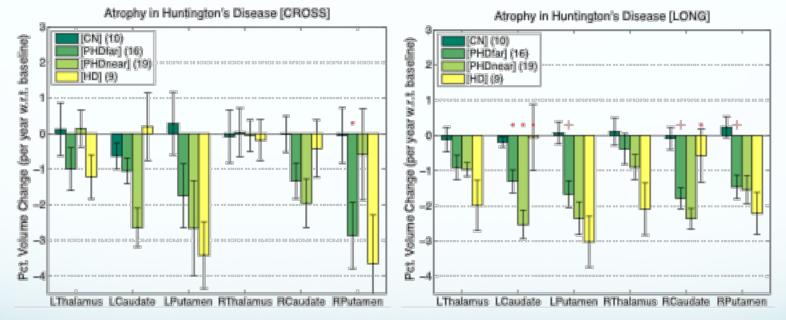


Sample Size Reduction when using [LONG] (based on test-retest 14 subjects, 2 weeks)

Huntington's Disease (3 visits) (with D. Rosas)

Independent Processing

Longitudinal Processing

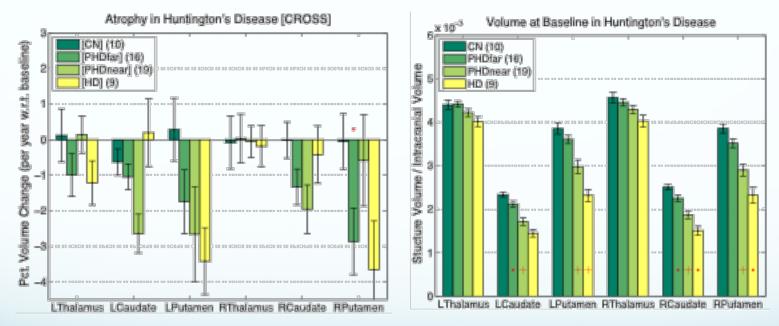


[LONG] shows higher precision and better discrimination power between groups (specificity and sensitivity).

Huntington's Disease (3 visits) (with D. Rosas)

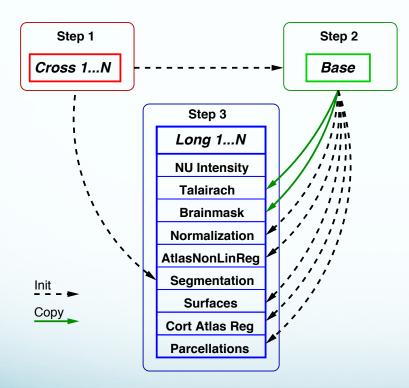
Rate of Atrophy

Baseline Vol. (normalized)



Putamen Atrophy Rate can is significantly different between CN and PHD far, but baseline volume is not.

Robust Template for Initialization



- Unbiased
- Reduces Variability
- Common space for:
 - TIV estimation
 - Skullstrip
 - Affine Talairach Registration
- Basis for:
 - Intensity Normalization
 - Non-linear Registration
 - Surfaces / Parcellation

FreeSurfer Commands (recon-all)

1.CROSS (independently for each time point tpNid):

recon-all -subjid tpNid -all

2. BASE (creates template, one for each subject):

recon-all -base baseid -tp tp1id \ -tp tp2id ... -all

3. LONG (for each time point tpNid, passing baseid):

recon-all -long tpNid baseid -all

This creates the final directories tpNid.long.baseid

Directory Structure

Contains all CROSS, BASE and LONG data:

- me1
- me2
- me3
- me_base
- me1.long.me_base
- me2.long.me_base
- me3.long.me_base
- you1

. . .

Single time point

Since FS5.2 you can run subjects with a single time point through the longitudinal stream!

- Mixed effects models can use single time point subjects to estimate variance (increased power)
- This assures identical processing steps as in a subject with several time points
- Commands same as above:

```
recon-all -subjid tp1id -all
recon-all -base baseid -tp tp1id -all
recon-all -long tp1id baseid -all
```

Final Remarks ...

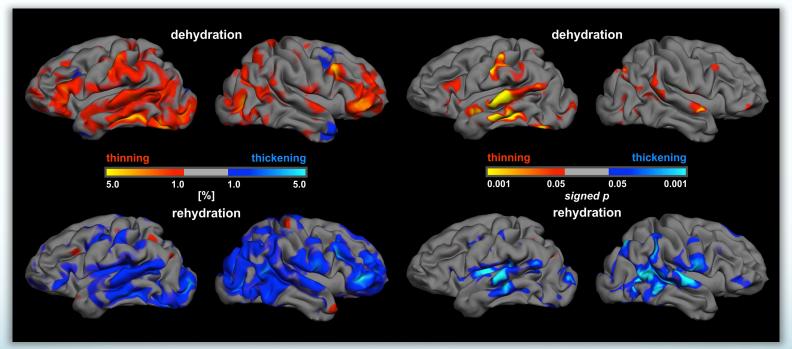
Sources of Bias during Acquisition

BAD: influence images directly and cannot be easily removed!

- Different Scanner Hardware (Headcoil, Pillow?)
- Different Scanner Software (Shimming Algorithm)
- Scanner Drift and Calibration
- Different Motion Levels Across Groups
- Different Hydration Levels (season, time of day)

Hydration Levels

14 subjects, 12h dehydration (over night)



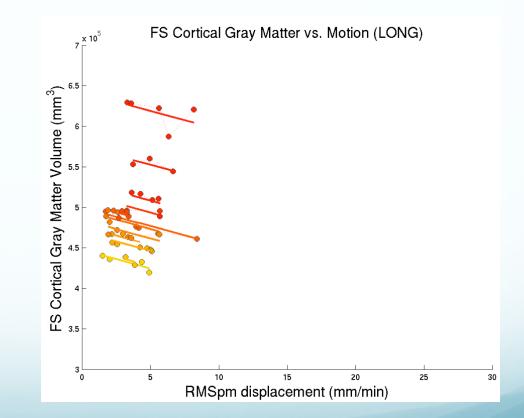
rehydration 1L/h

Biller et al. American Journal of Neuroradiology 2015

Motion Biases GM Estimates

- 12 volunteers
- 5 motion types:
 - 2 Still
 - Nod
 - Shake
 - Free
- Duration:
 - 5-15 s/min

Effect: roughly 0.7-1% volume loss per 1mm/min increase in motion



Still to come ...

- Common warps (non-linear)
- Optimized intracranial volume estimation
- Joint intensity normalization
- New thickness computation
- Joint spherical registration

http://freesurfer.net/fswiki/LongitudinalProcessing http://reuter.mit.edu/publications

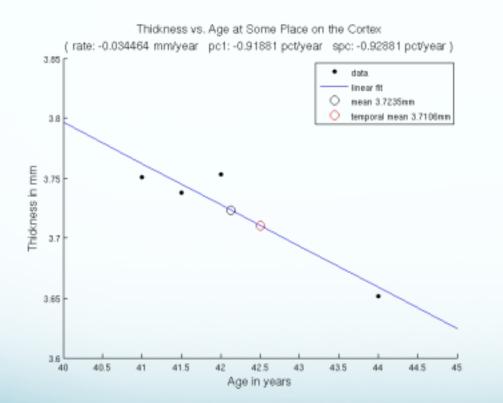
Thanks to: the FreeSurfer Team

Longitudinal Tutorial

Longitudinal Tutorial

- 1. How to process longitudinal data
 - Three stages: CROSS, BASE, LONG
- 2. Post-processing (statistical analysis):
 - (i) compute atrophy rate within each subject
 - (ii) group analysis (average rates, compare)
 - here: two time points, rate or percent change
- 3. Manual Edits
 - Start in CROSS, do BASE, then LONGs should be fixed automatically
 - Often it is enough to just edit the BASE
 - See <u>http://freesurfer.net/fswiki/LongitudinalEdits</u>

Longitudinal Tutorial



- Temporal Average
- Rate of Change
- Percent Change (w.r.t. time 1)
- Symmetrized Percent Change (w.r.t. temp. avg.)